Optical heart rate monitoring – OHRM
based on X-NUCLEO-IKA01A1 expansion board

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Main components

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<th>Component</th>
<th>Description</th>
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<tr>
<td>TSU104</td>
<td>Nanopower, rail-to-rail input and output, 5 V CMOS operational amplifiers</td>
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<tr>
<td>BlueNRG-MS</td>
<td>Upgradable Bluetooth® Low Energy network processor</td>
</tr>
<tr>
<td>STM32L053R8</td>
<td>Ultra-low-power ARM Cortex-M0+ MCU with 64 Kbytes Flash, 32 MHz CPU, USB, LCD</td>
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Purpose and benefits

The X-NUCLEO-IKA01A1 is a multifunctional board based on ST operational amplifiers and it embeds several configurations. In this design tip we will use two of them to build an optical heart rate monitor (OHRM).

We will also show how to connect BLE expansion board X-NUCLEO-IDB05A01 to the heart rate monitor and how to send data to your smartphone. This design tip will make it easier to build a prototype of your own wearable optical heart rate monitor.

Description

Introduction to OHRM

Optical heart rate monitoring is a simple method to determine one's heart rate without using electrodes. It uses the optical characteristics of hemoglobin, which attenuates light based on the concentration of oxygen in the blood. Each time the heart beats, it brings fresh blood with oxygen to the muscles. The muscles use the oxygen and decrease its concentration. Therefore we are able to determine the heart rate from the time dependency of oxygen concentration in the blood.

This simple principle can give us heart rate, but cannot measure the level of oxygen directly. To measure the oxygen concentration we need to add a second light source with a different wavelength. Thanks to this method, it is possible to determine peripheral oxygen saturation. This principle is called pulse oximetry and is commonly used in medical heart rate monitoring.
The LEDs are used to emit light through the skin. Hemoglobin has the highest attenuation for red light, so it is good to use it but green or infrared light can be used as well. The sensing element is usually a photodiode.

Building the system

To build a complete optical heart rate monitor we need to know how to do signal conditioning and which boards can be used. The overall block diagram of the system is shown in Figure 1.

Figure 1. Block diagram of the optical heart rate monitor
Hardware modifications

In order to build the optical heart rate monitor using the X-NUCLEO-IKA01A1 expansion board stacked on the NUCLEO-L053R8 board, some modifications are required.

**X-NUCLEO-IKA01A1 modifications**

The X-NUCLEO-IKA01A1 expansion board doesn’t contain an infrared (IR) LED for emitting light, therefore it must be added. The recommended specifications of the LED are:

- 3 mm or 5 mm through-hole type
- Wavelength $\lambda$ from 850 nm to 1000 nm
- High forward current

Solder the IR LED to pins LED_A and LED_K on the X-NUCLEO-IKA01A1 expansion board. Be aware of the polarity of the diode.

Figure 2. Pins to solder IR LED on X-NUCLEO-IKA01A1

**X-NUCLEO-IDB05A1 modifications**

If you want to use a BLE extension module to transfer heart rate data, you need to make some modifications to this board as well.

- Remove resistors R1, R2 and R4
- Put 0R resistors on R6, R7 and R8

Note that libraries for use with the X-NUCLEO-IDB05A1 cannot deal with this modification automatically and the settings of the pins and its alternate function must also be changed. When using the X-CUBE-BLE1, the SPI pin settings can be found in:

`stm32l0xx_nucleo_bluenrg.h` header file.
Signal conditioning

Driving the LED

The PWM current driver available on X-NUCLEO-IKA01A1 can be used to drive the LED. It is not necessary to drive the LED by exact current in this application, and a simple transistor driven from the MCU can be used.

Figure 3. Light of IR LED soldered to X-NUCLEO-IKA01A1 seen through digital camera

Analog amplifier

The photodiode generates very small current which needs to be amplified. This current is in the range of tens of micro amps but the useful signal generated by heartbeats is only in the range of hundreds of nano amps. To amplify such a small currents we need to use a transimpedance amplifier (TIA) with the right operational amplifier. You can see the structure of this amplifier below.

Figure 4. Transimpedance amplifier structure
The amplification of small currents brings some constraints to the op-amp used. The input bias current of the op-amp input should be much lower than the smallest signal we are interested in. In this case it means that input bias current should be lower than hundreds of pico amps.

The heartbeats are relatively slow. Considering the maximal human heartbeat being 180 bpm, the maximal frequency of interest is 3 Hz and therefore there are no constraints on the bandwidth of the op-amp.

Last and possibly the most important is power consumption. Wearable devices are always powered by batteries so we need to select an op-amp with the lowest possible power consumption.

Taking into account all these constraints we find that the best op-amp is TSU104:

- Submicro ampere current consumption: 580 nA typ per channel at 25 °C at VCC = 1.8 V
- Low supply voltage: 1.5 V - 5.5 V
- Gain bandwidth product: 8 kHz typ
- Low input bias current: 5 pA max at 25 °C

**Digital signal processing**

Output from the trans-impedance amplifier can be directly used to drive the ADC. Unfortunately, the sampled data is full of noise coming from movement and ambient light, and it contains a huge DC part which we are not interested in.

Figure 5. Block diagram of digital signal processing

To get rid of ambient light we can use the light modulation technique. Measurement is done twice, first with the LED turned on, and a second time with it turned off. Subtracting these values will give us only the contribution of the LED. Note that the time delay between the samples must be as short as possible.

Another source of unwanted signals is indoor lights. Most of these lights flicker with a frequency of 100 Hz or 120 Hz in North America. It is not possible to avoid this signal but it is possible to use the right sampling frequency to take the flickers out of the range of interest. The recommended sampling rate of the ADC is in range from 30 sps to 43 sps. Note that the higher sampling frequency means more taps in the digital filter to obtain a similar frequency response, and therefore more processing power may be needed.
To cancel the rest of the unwanted signals, we need to employ filtration. One of the easiest ways is to use a FIR filter designed as a band pass filter in the range of 0.5 Hz to 3 Hz. The measured signals can be seen in Figure 6.

Figure 6. Graph showing data during signal processing

In this graph, the heartbeats can be clearly recognized in the filtered signal. A simple peak detection method can be used. To achieve better accuracy and more stable output it is recommended to use another algorithm to determine if the measured bpm is valuable. One of these can be median filtration. It is also good to count with the dynamic of heart rate.
BLE extension

Measured heart rate data can be directly sent to your smart device. Bluetooth low energy has a standard communication profile for heart rate monitoring. This profile is also supported by ST BlueNRG-MS device.

Figure 7. Prototype of heart rate monitor

Conclusion

Optical heart rate monitoring is known as a part of medical pulse oximeters. As the wearable application segment grows, the simplified configuration of pulse oximeters will gain popularity. By embedding optical heart rate monitoring into smart watches or fitness trackers, health monitoring becomes easier.

The TSU104 nanopower quad 5 V CMOS op-amp with rail-to-rail input and output is used for analog signal conditioning.
Support material

List of support materials and documents related to this design tip

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Documentation

Datasheet: TSU104, Nanopower, rail-to-rail input and output, 5 V CMOS operational amplifiers

User manual: UM1955, Getting started with the multifunctional expansion board based on operational amplifiers for STM32 Nucleo

Revision history

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<tr>
<td>04-Oct-2016</td>
<td>1</td>
<td>Initial release</td>
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