

Ultrasound Pulsers for Non-Destructive Testing and Medical Imaging Applications

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Presentation Outline

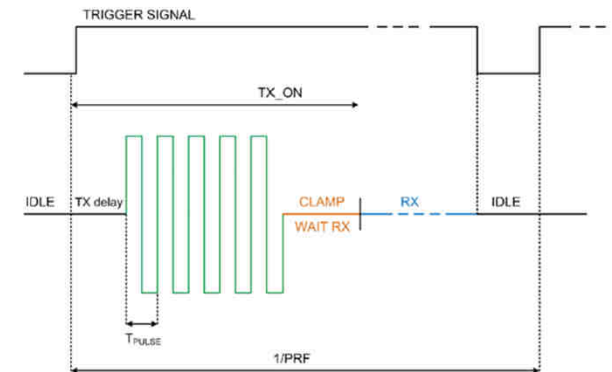
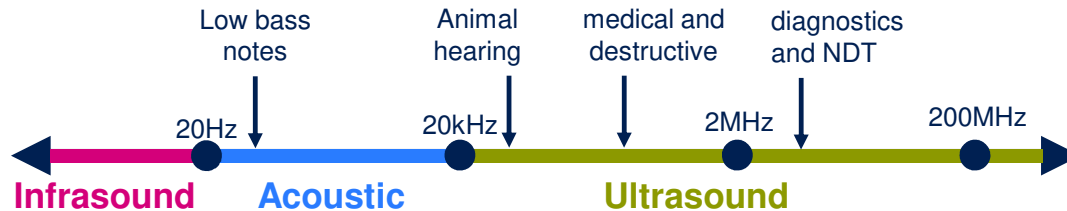
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- Ultrasound physics:
 - Ultrasound waves
 - Propagation
 - Transducers
 - Beamforming
 - Doppler effect
- Applications:
 - Medical application
 - NDT application
- System and Products:
 - System Architecture
 - ST portfolio

Ultrasound Waves

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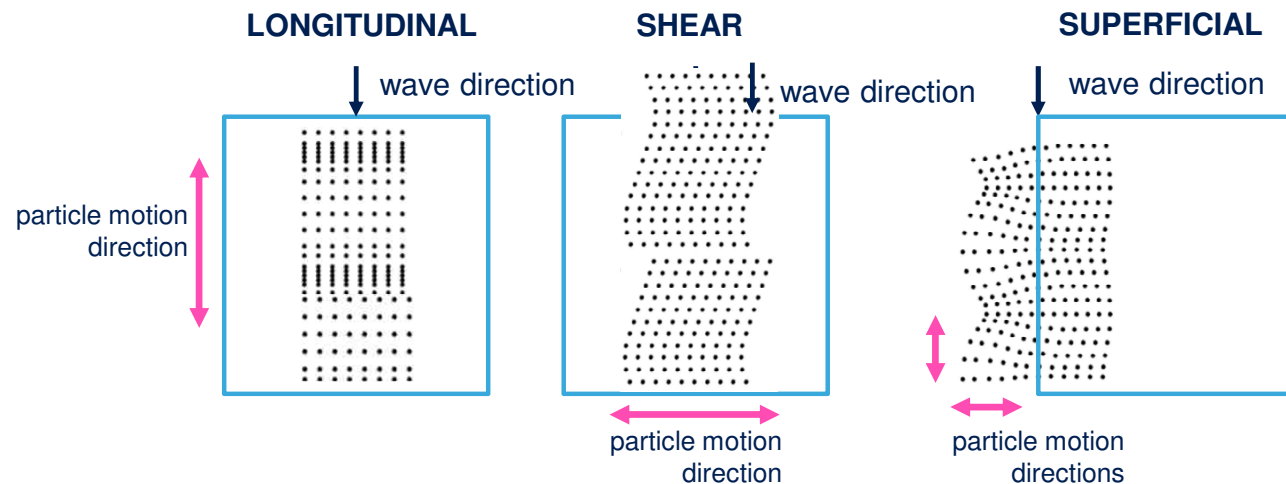
- Sound is a mechanical wave (acoustic wave) coming from a vibrating object, propagating in an elastic medium (solid, liquid or gas) through particle collision
- Ultrasound is a sound wave with frequency above the audible range limit of human hearing (over 20KHz). Standard application frequencies are 500kHz - 20MHz.
- From the physical point of view, an ultrasound wave is not different from an acoustic wave



Ultrasound Wave Propagation

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- Longitudinal wave: expansion and compression, particles moving from rest position in the same direction of wave propagation. It can propagate in solid, liquid or gas.
- Shear (transverse) wave: particle vibrations are perpendicular to the wave direction. Speed is lower (about half) than longitudinal wave. It can propagate only in solid mediums.
- Superficial wave: the oscillating motion travels along the surface to a depth of one wavelength; the particle movement is a combination of longitudinal and transverse motion, creating an elliptic pattern of motion. Superficial waves follow the surface profile. It can propagate in solid materials.



Main Parameters

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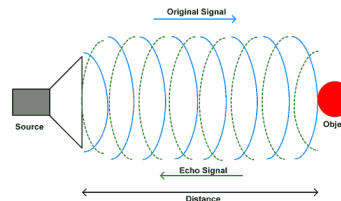
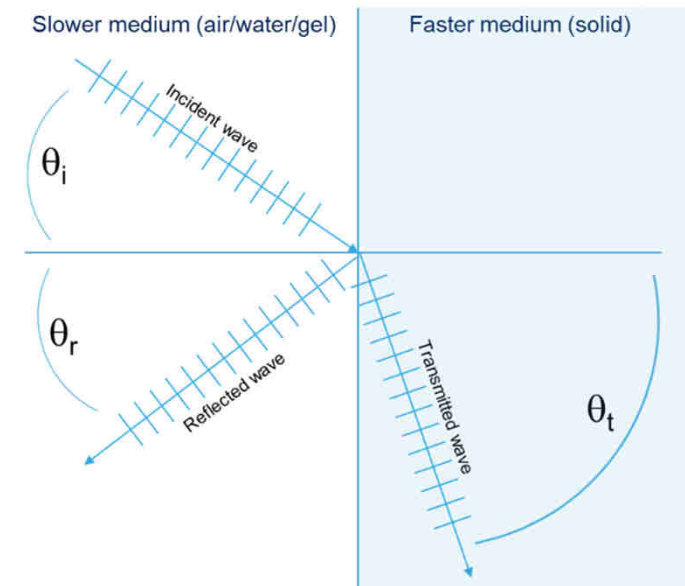
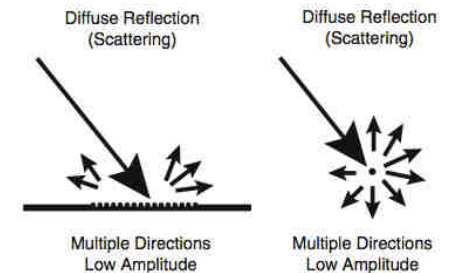
- T [s]: time between two maximums of the waveform (Period)
- v [m/s]: waveform speed, it depends on the material properties (elasticity k and density ρ) where $v = \sqrt{k/\rho}$.
- λ [m]: waveform length. It is the ratio v/f
- α : medium attenuation, used to calculate the wave attenuation vs. penetration $A(x) = A_0 e^{-\alpha x}$
 - Absorption is the transformation of Ultrasound energy in thermal energy
 - Diffusion is the beam dispersion, attenuation in the propagation direction
- Z : acoustic impedance, $Z = \rho \cdot v$. It is the resistance to the ultrasound wave propagation. Impedance mismatch is the cause of scattering, transmission and reflection

Medium	v [m/s]	ρ [kg/m ³]	Z [MRayl]
Air	330	1.2	0.0004
Water	1480	1000	1.48
Aluminum	6320	2700	17.06
Bronze	3530	8860	31.27
Copper	4660	8930	41.60
Iron	5900	7700	45.43
Lead	2160	11400	24.62
Silver	3600	10500	37.80
Titanium	6070	4500	27.31
Blood	1584	1060	1.68
Bone, Cortical	3476	1975	7.38
Cardiac	1576	1060	1.67
Connective Tissue	1613	1120	1.81
Muscle	1547	1050	1.62
Soft tissue	1561	1043	1.63

Scattering, Reflection & Transmission

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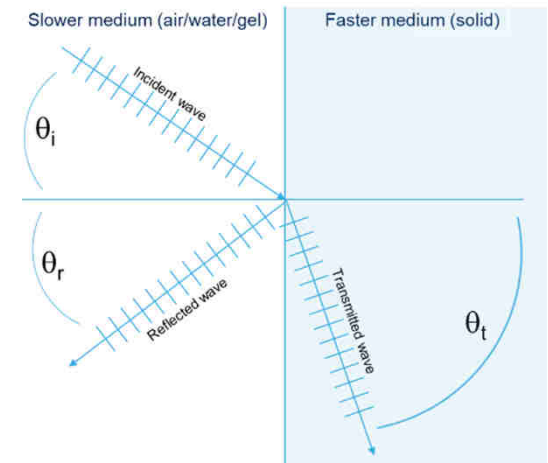
- Scattering: the energy lost when the wave propagates onto a medium interface whose irregularities are comparable with λ (the two mediums must have different acoustic impedance)
- Reflection/Transmission: when an incident wave propagates onto an interface larger than λ , the “ray approximation” can be used.
- The reflected wave is the *echo*



Transmission and Reflection 7

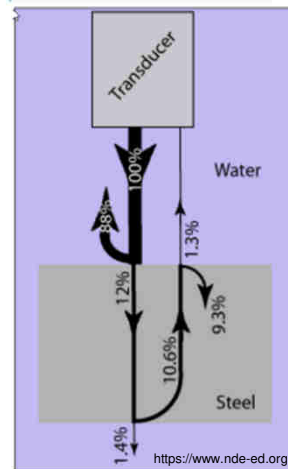
- Angle of refraction is defined by Snell's law:
- The angle of reflection is equal to the incident angle
- The fraction of transmitted and reflected energy depends on the acoustic impedance (Z) and incidence angle (θ). The greater the impedance mismatch, the greater the percentage of energy that will be reflected at the interface or boundary between one medium and another

$$\frac{\sin \theta_I}{c_1} = \frac{\sin \theta_T}{c_2}$$



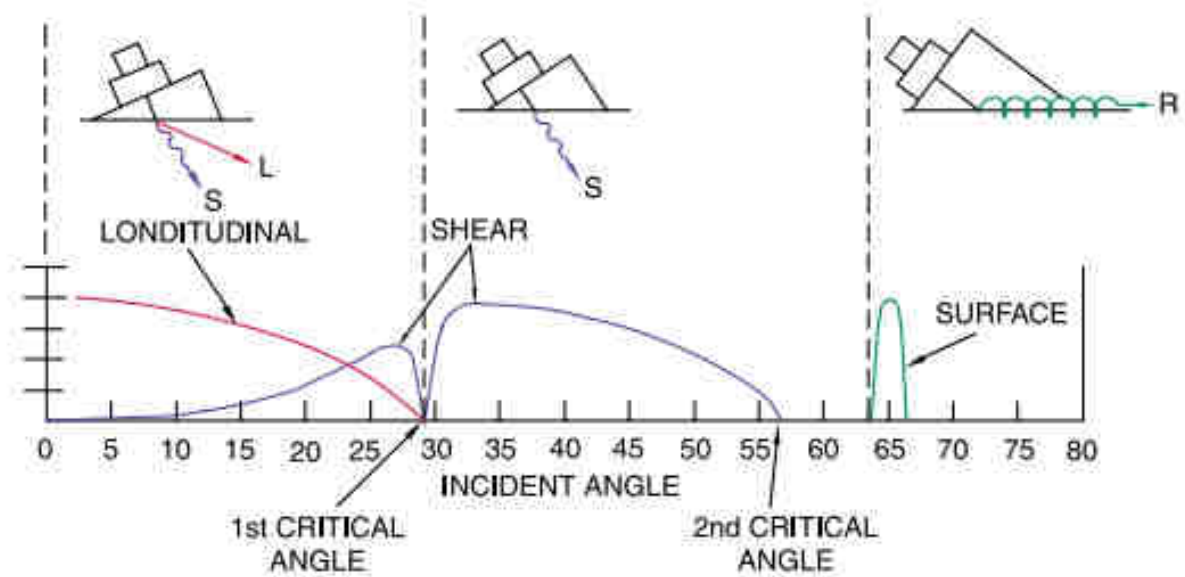
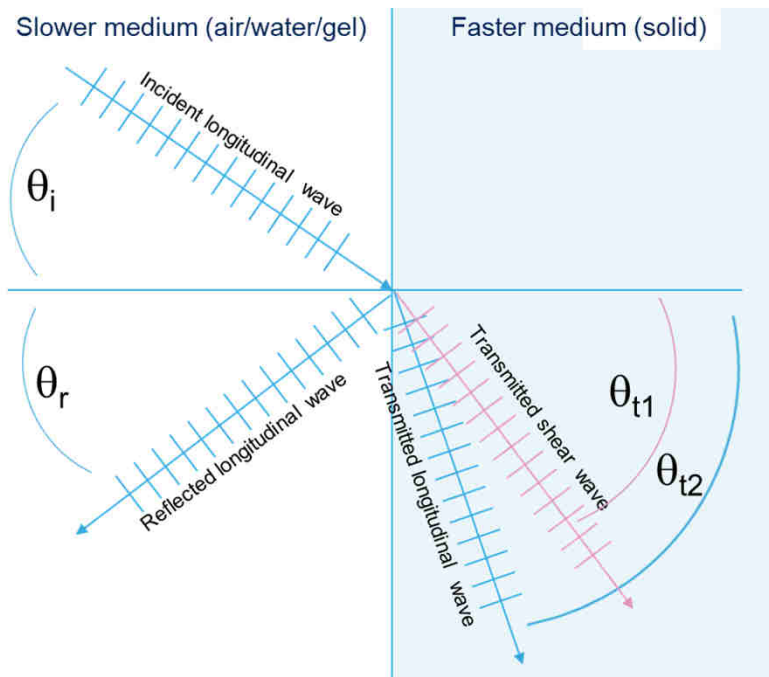
$$R = \frac{(Z_2 \cos \theta_i - Z_1 \cos \theta_t)^2}{(Z_1 \cos \theta_t + Z_2 \cos \theta_i)^2}$$

$$T = 1 - R = \frac{(4Z_1 Z_2 \cos \theta_i \cos \theta_t)^2}{(Z_1 \cos \theta_t + Z_2 \cos \theta_i)^2}$$



Critical angle of incidence

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<http://www.sdindt.com/>

Ultrasonic Transducers

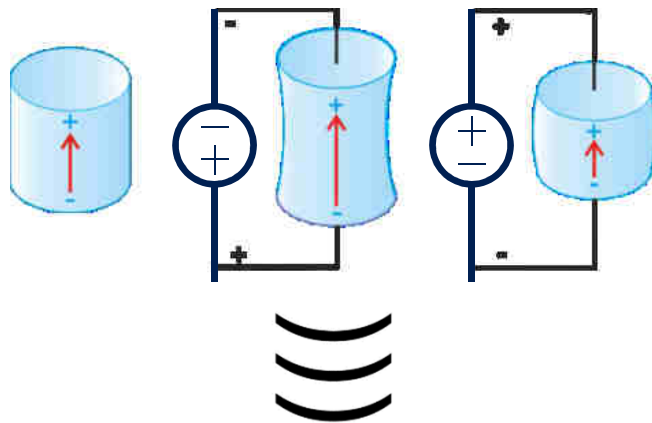
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Piezoelectric transducer

- based on misalignment of the dipoles

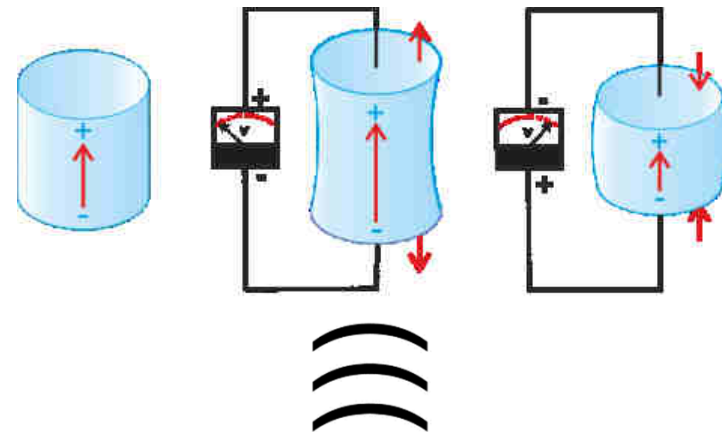
Transmission (TX) mode

Forcing a voltage on a piezoelectric material, it contracts or expands proportionally to the applied voltage



Receiving (RX) mode

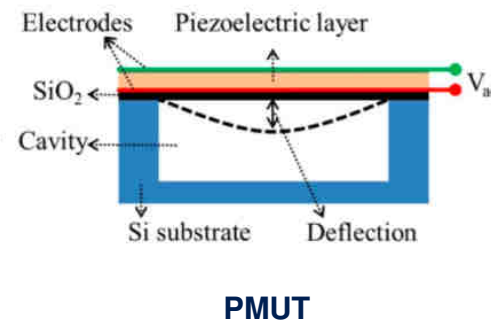
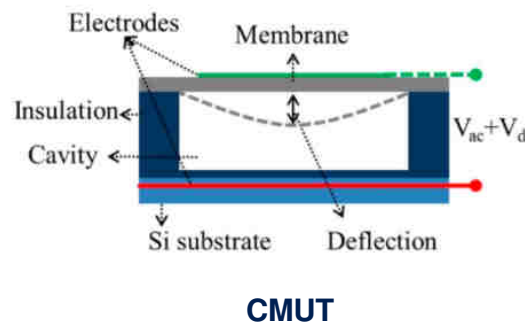
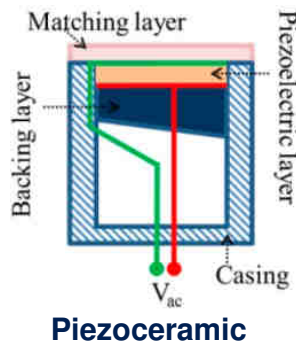
Forcing a mechanical stress on a piezoelectric material, it generates an electric field



Transducer Types 10

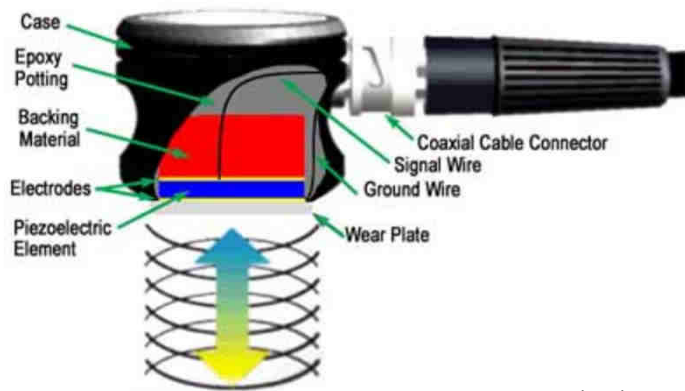
- An Ultrasound transducer is a material able to convert electrical energy into mechanical vibrations (ultrasound wave) and vice versa.
- Mainstream industrial solutions:
 - Piezoceramic (PZT, lead zirconate titanate)
 - CMUT (Capacitive Micro machined Ultrasound Transducer)
 - PMUT (Piezoelectric Micro machined Ultrasonic Transducers)

Parameters	PIEZOCERAMIC	CMUT	PMUT
Bandwidth	narrow	wide	wide
Linearity	high	low	low
Sensitivity	high	medium	low
Cost	high	low	Medium/low
Dimension	large	small	small
HV bias in RX	no	yes	no

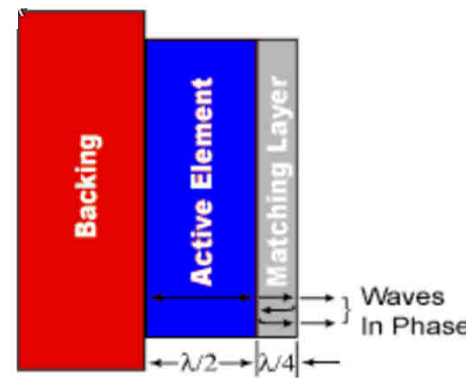


Physical Structure of Piezo Transducers

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www.nde-ed.org



Backing material: absorbing material used to increase beam penetration (on back side)

Active element: Piezoelectric material, whose dimension depend on wave characteristic

Matching Layer: material used to improve the coupling between active element and the medium

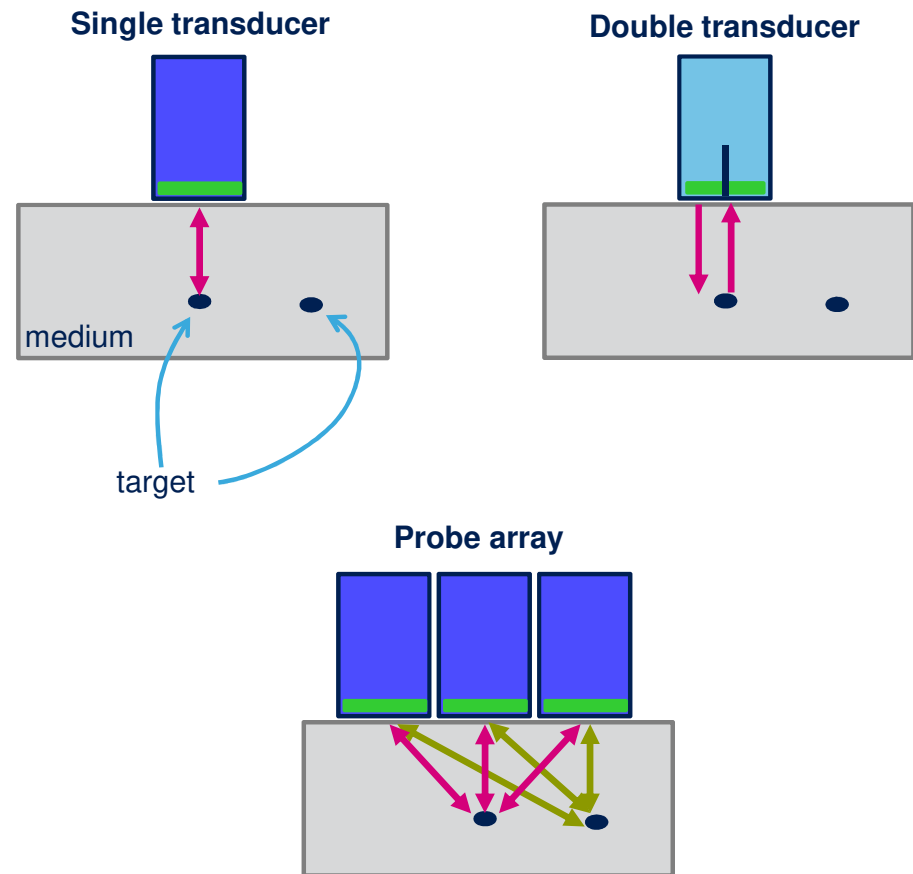
Transducer main characteristics:

- Physical dimensions
- Resonant frequency:
 - low frequency \rightarrow lower resolution / higher penetration;
 - high frequency \rightarrow higher resolution / lower penetration

Transducer arrangement

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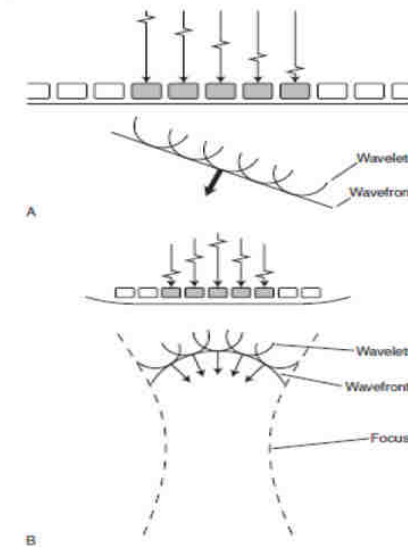
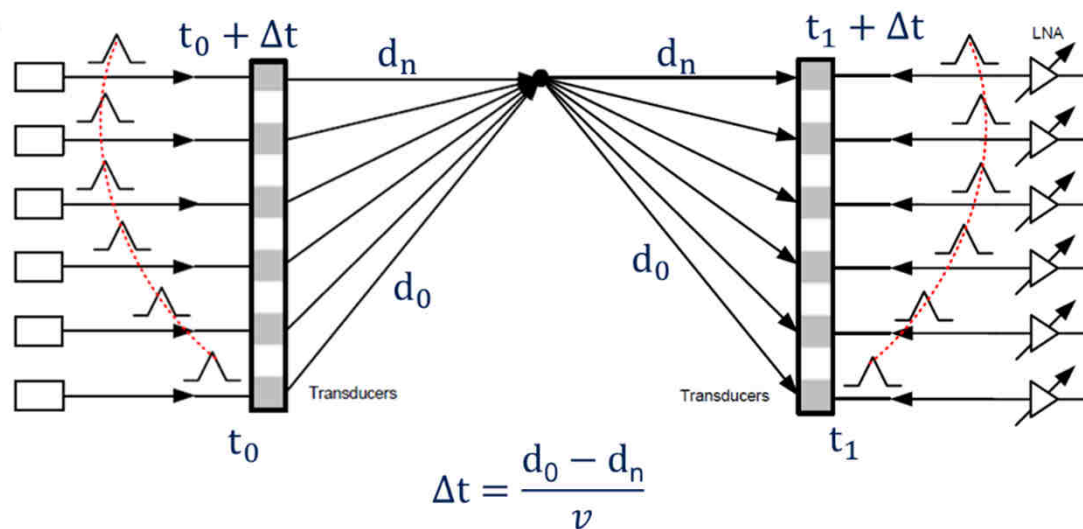
- Single transducer
 - Used for both RX and TX
 - Alternate phases (TX, wait, RX)
- Double transducer
 - Dedicated transducer for TX
 - Dedicated transducer for RX
 - Continuous analysis
- Probe array
 - More elements side-by-side
 - Dynamic focusing (beamforming)



Beamforming

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- In a probe array application, a delay profile can be used to maximize the energy sent in particular area in TX
- The delay is important also in RX to realign the echo and improve SNR



Beam steering

Beam focusing

Doppler Effect

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The reflected wave from a moving obstacle shows a frequency shift proportional to the obstacle speed

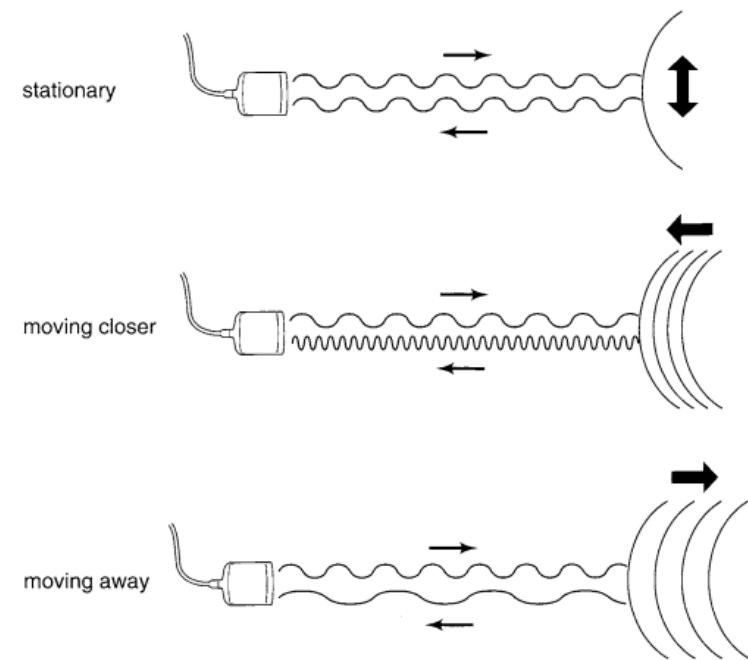
$$\Delta f = 2 \frac{v \cos \theta}{c} f_0$$

$v \cos \theta$: target speed component in the wave propagation direction

c : wave speed

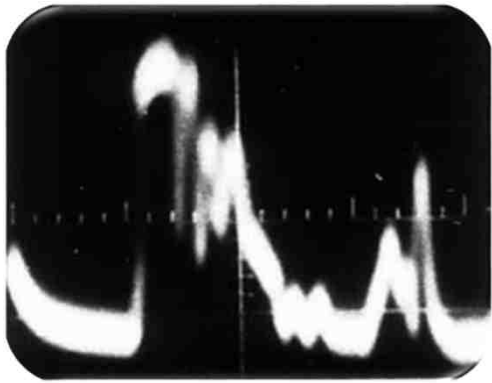
f_0 : wave frequency

- The frequency shift is due to the Doppler effect
- Positive or negative depending on the direction of motion
- Doppler mode has no imaging capability

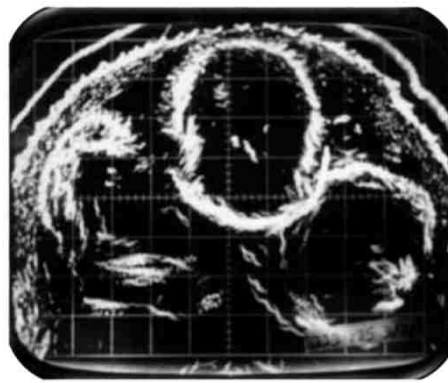


Ultrasound and Medical Imaging

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Early '50: A-mode (amplitude) image



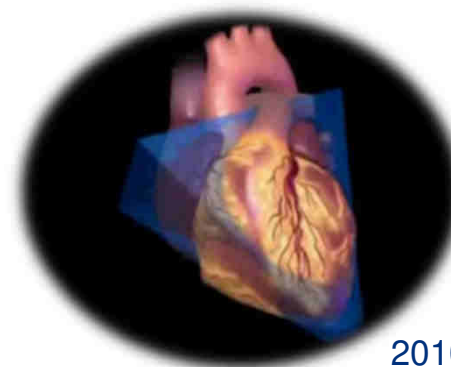
Late '50: B-mode (brightness) static image



'60: real time B-mode imaging



2000: 3D ultrasound imaging



2010: 4D ultrasound imaging

Ultrasound NDT application

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Non-Destructive Testing (NDT) is a technology used to detect defects in materials and structures, either during manufacturing or while in service (cracks, slag, porosity, stringers, ...).

Air or cracks represent a reflector with different acoustic impedance

- By analyzing these reflections it is possible to measure the thickness of a test piece, or find the location of internal flaws.
- Amplitude, frequency and delay of echoes are related to position, speed, material composition and geometry of the target

Ultrasound NDT works with a large number of materials:

- Metals, plastics, ceramics...
- Biological tissue
- It doesn't work well in wood



Inspection Methodologies

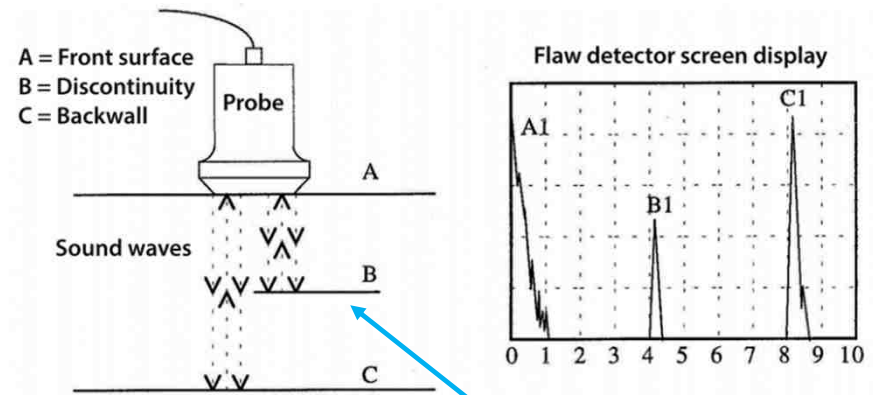
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- Normal beam inspection:

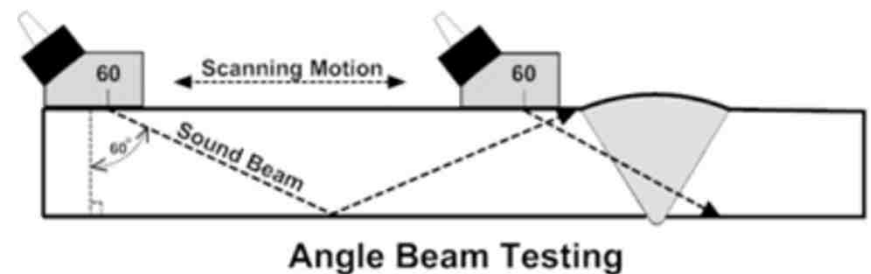
- Longitudinal wave
- Perpendicular to surface
- Not useful on welded areas

- Angle beam inspection:

- Refracted shear wave (high incident angle to remove longitudinal wave)
- Variable angle between transducer and surface
- Works on area with no irregular surface (welded areas)

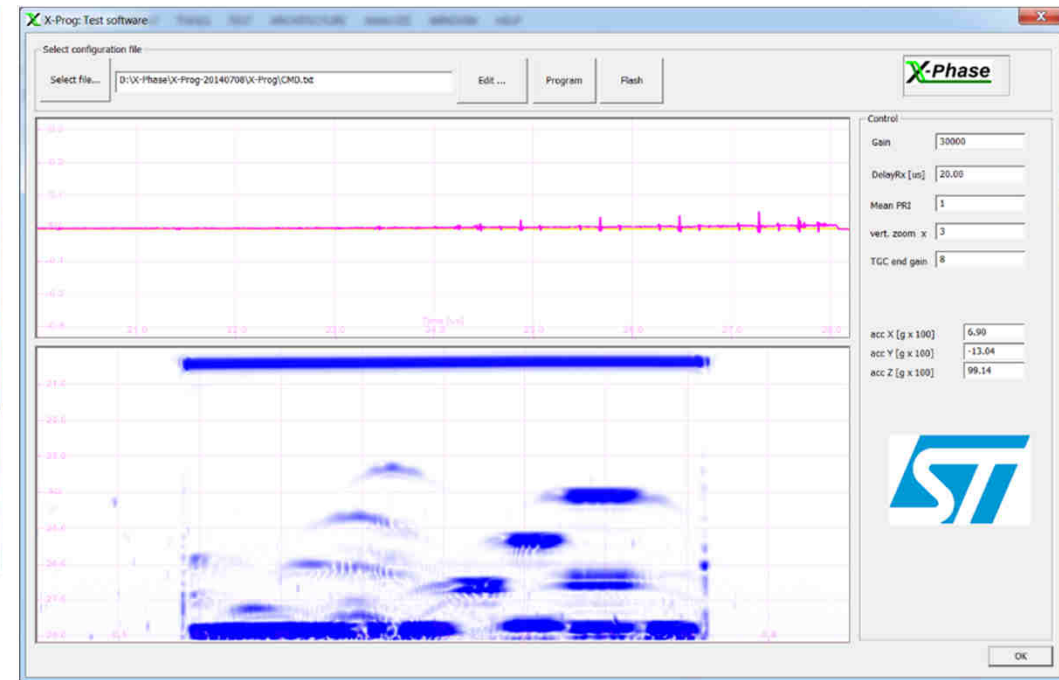
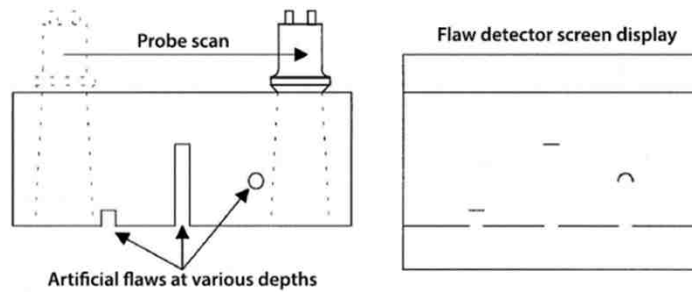
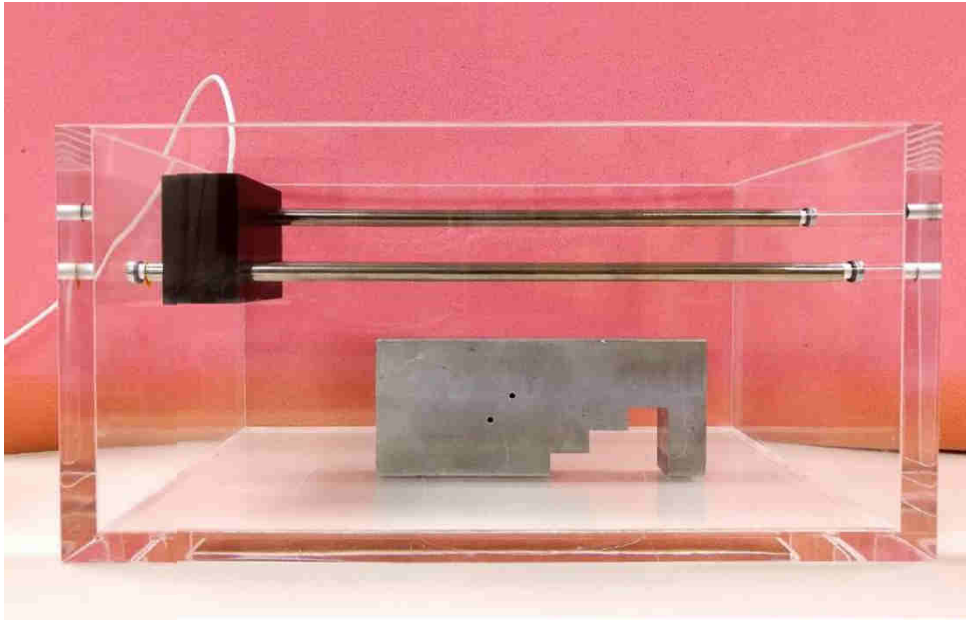


Not able to see under first flaw



Ultrasound NDT Demo

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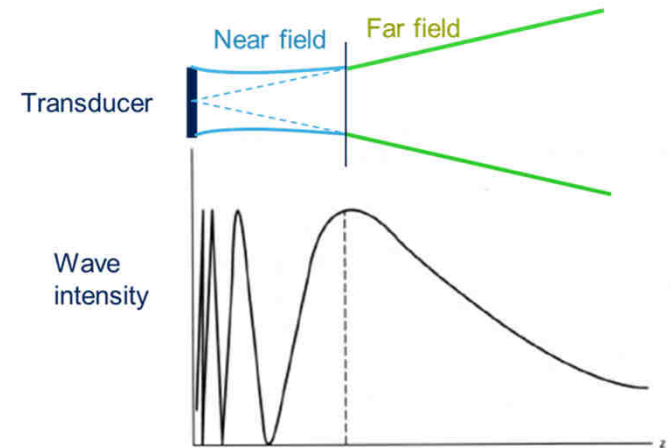
Ultrasound vs. other NDT Technologies 19

Parameters	Visual	X-ray	Eddy current	Magnetic particle	Liquid penetrant	Infrared thermography	Ultrasonic
Testing cost	low	high	low/medium	medium	low	high	very low
Time consuming	short delay	delayed	immediate	short delay	short delay	short delay	immediate
Possible to automate	no	fair	good	fair	fair	good	good
Portability	high	low	high/medium	high/medium	high	low	high
Type of defect	External	all	external	external	Surface breaking	internal	internal
Thickness gauging	no	yes	yes	no	no	yes	yes
Effect of surface geometry	Negligible	significant	significant	negligible	negligible	negligible	significant

Quality Parameters

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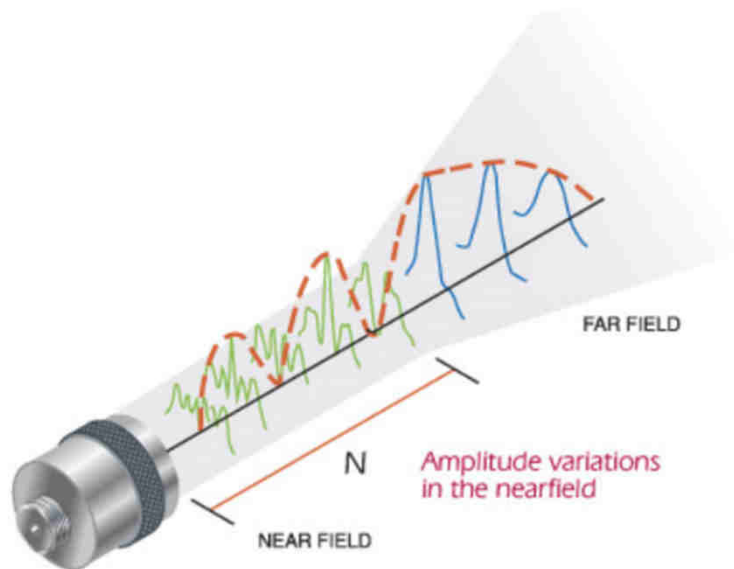
- **Sensitivity** is the ability of a system to detect reflectors at a given depth. The greater the signal that is received from these reflectors, the more sensitive the transducer system.
- **Resolution** is the ability of a system to detect separate echoes from reflectors placed near to each other.
 - **Axial resolution:** Smallest detail that can be seen in the direction of propagation, it is equal to λ so it depends on frequency (higher frequency, higher resolution) ($\pm 1\mu\text{m}$ @ 1MHz)
 - **Lateral resolution:** Smallest detail that can be seen in the direction perpendicular to the propagation axis. It depends on frequency, transducer width, focusing capability.
 - **Near surface resolution** is the ability of the ultrasonic system to detect reflectors located close to the surface



	High frequency signal	Low frequency signal
Attenuation	HIGH	LOW
Penetration	LOW	HIGH
Resolution	HIGH	LOW

Near Field and Far Field

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www.olympus-ims.com

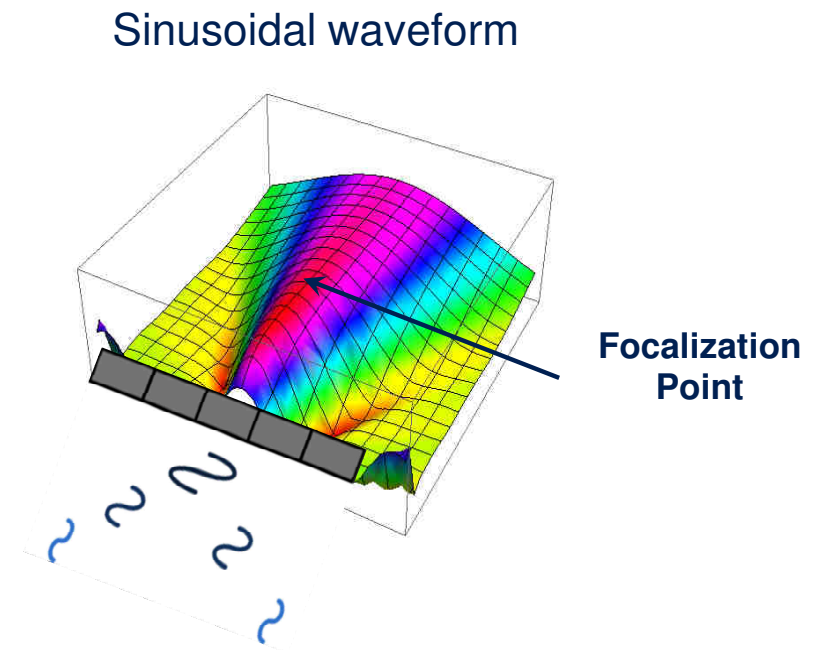
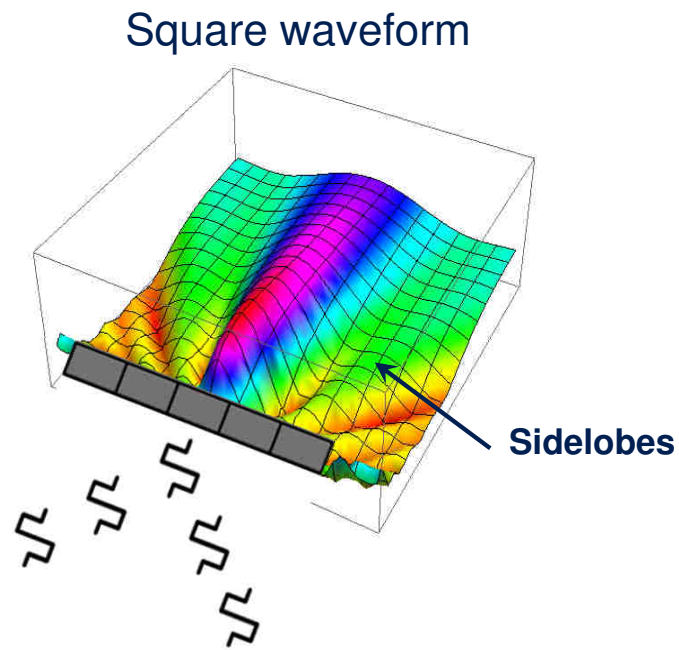
Ultrasound wave intensity along the beam is not constant because of transducer finite dimension

- Near field: zone close to active element.
 - Extensive fluctuations in the sound intensity
 - Difficult evaluate flaws in this zone
- Far field: zone far to active element.
 - Beam is more uniform
 - Beam spreads out
 - Good detection
- Natural focus is the distance between far and near field.
- Natural focus is the distance where sound wave have the maximum strength

Signal Excitation

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Acoustic
Pressure
In transmission

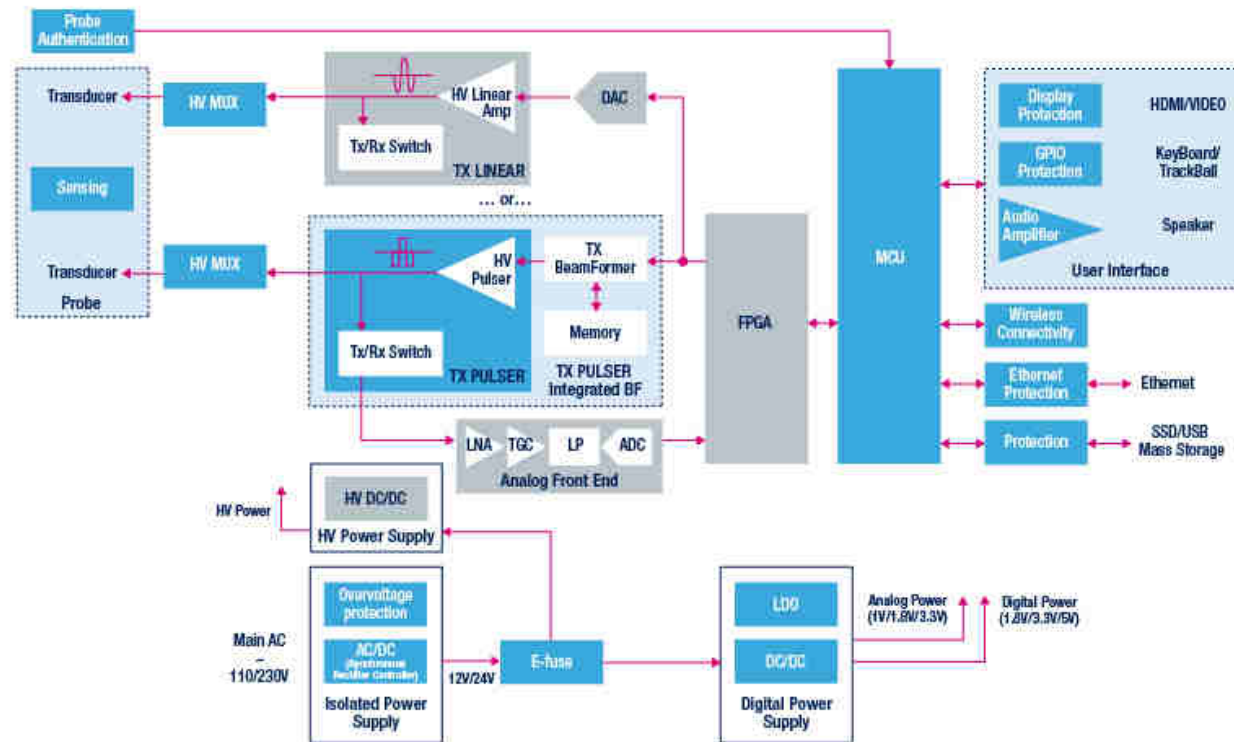


ST Ultrasound Pulsers

Medical Ultrasound

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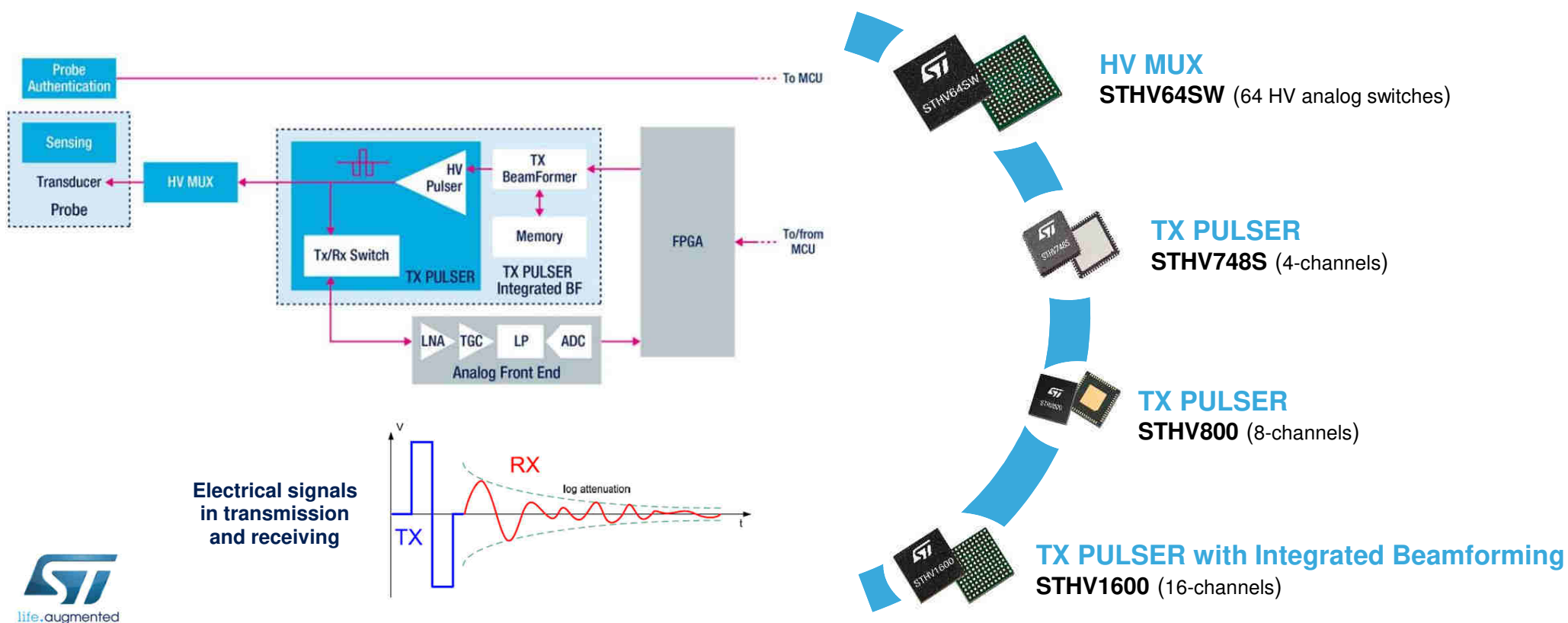
ST technologies for Ultrasound: from Standard Products to Application Specific ICs

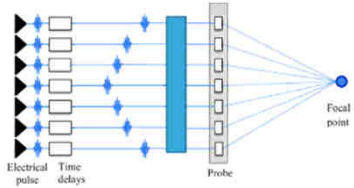


Medical Ultrasound Partitioning

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High Voltage Stage and Smart Probe





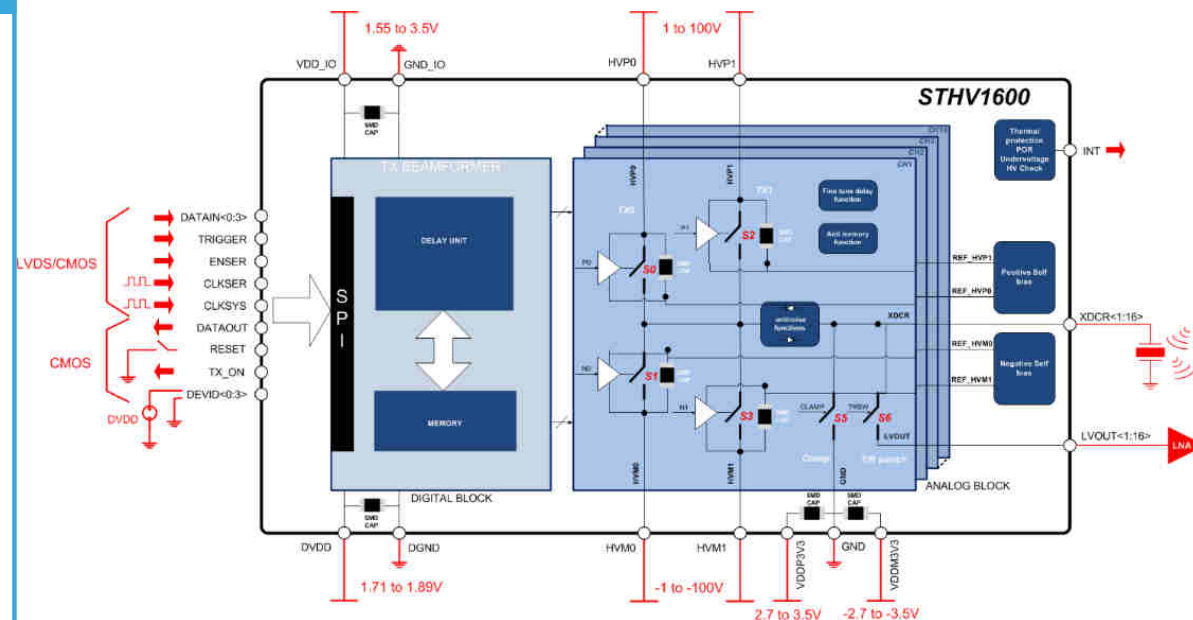
STHV1600

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16 channel Pulser with Beamforming

Monolithic 16 ch high-speed ultrasound pulser with integrated transmit beamformer

- 0 to 200V peak-to-peak output signal
- Up to 30MHz operating frequency
- Power-up/down sequence free
- Pulsed wave (PW) mode operation:
 - 5/3 RTZ level output, $\pm 2A$ / $\pm 4A$ source and sink
- Continuous wave (CW) mode operation
- Elastography mode operation
- Programmable delays to minimize 2nd harmonic distortion
- 11 Ω integrated active clamp to ground ($\pm 2A$)
- Integrated 9 Ω T/R switch
- **Digital Core**
 - TX Beamforming in transmission mode
 - Programmable single-channel delay
 - Clock frequency up to 200MHz
 - Delay from 0 to 327 μs with 5ns resolution
 - 65Kb embedded RAM to store patterns
 - Waveform compression algorithm
 - Control through serial interface (SPI)
- Package: TFBGA144 10x10x1.4mm

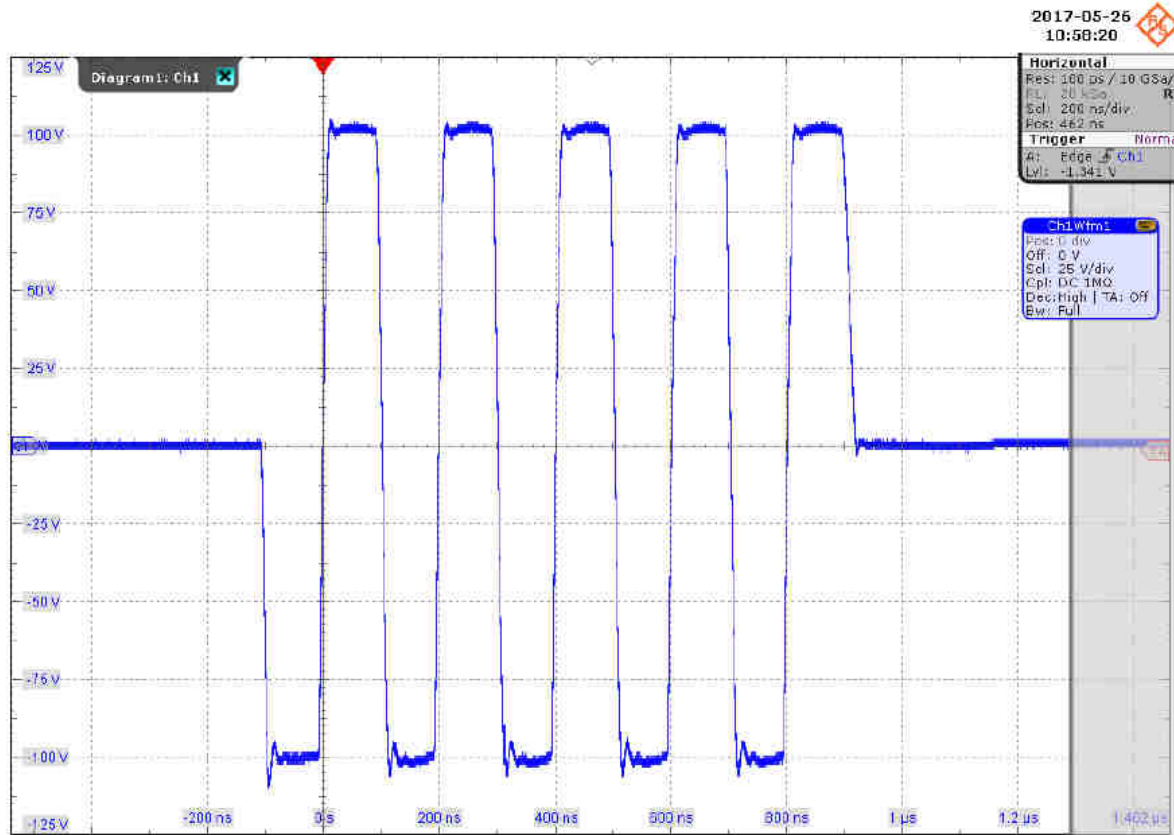


5 level PW mode



Pulse Wave operation

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Continuous Wave operation

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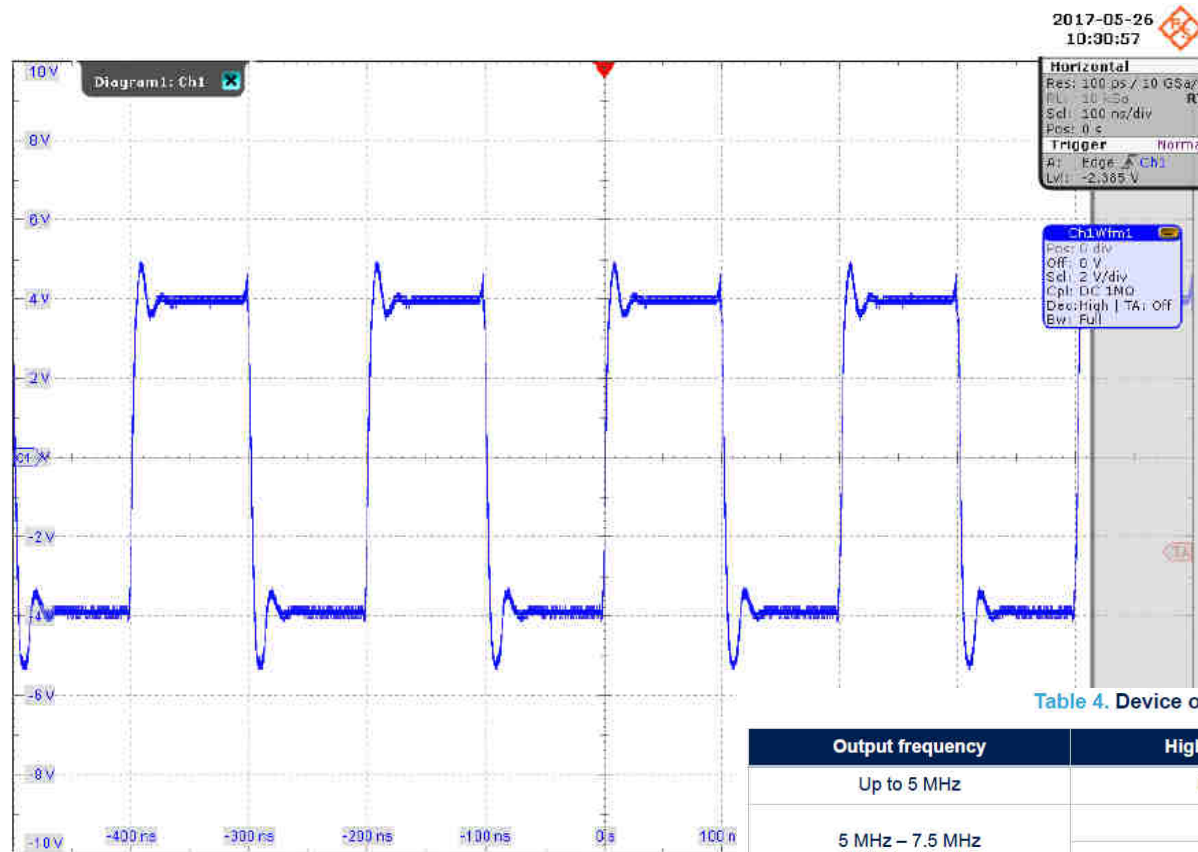


Table 4. Device overstress avoidance guidelines Elastography mode

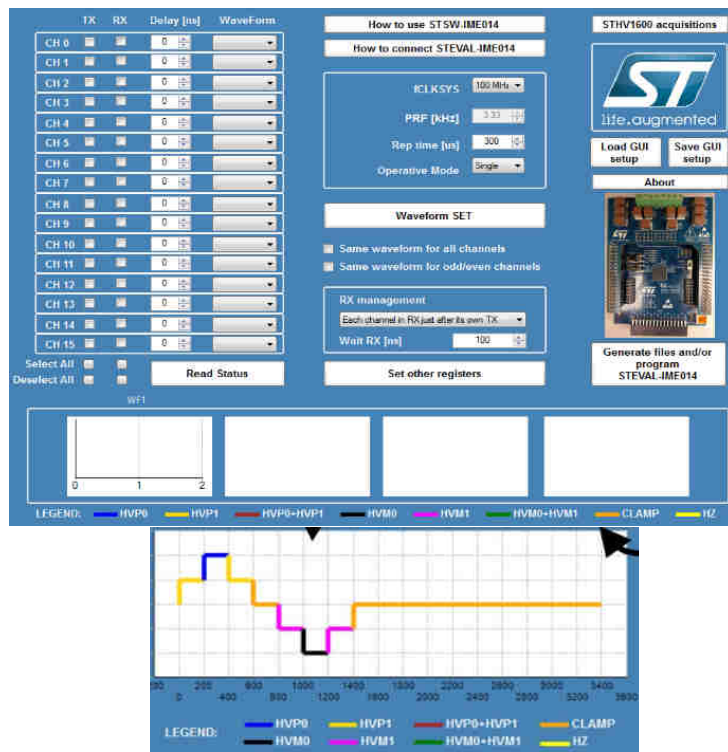
Output frequency	High voltage supply	Pulse train duration
Up to 5 MHz	Up to ± 100 V	Up to 1 ms
5 MHz – 7.5 MHz	Up to ± 90 V	Up to 1 ms
	± 100 V	Up to 750 μ s
7.5 MHz – 10 MHz	Up to ± 80 V	Up to 1 ms
	± 100 V	Up to 500 μ s

STHV1600 evaluation kit

STEVAL-IME014V1B

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GUI – HV waveforms builder



The kit consists of three connected modules:

- **Pulser module (STEVAL-IME014V1):**
 - STHV1600 16-channel pulser and buttons
 - Four preset programs and waveforms
 - USB interface to change programs and waveforms
 - Pushbutton interface to control waveform generation
 - Status LEDs
- **Power supply module (STEVAL-IME014V1D):**
 - Four high voltage and one low voltage supply lines
 - All low voltage supplies generated on-board
- **STM32 Nucleo microcontroller module:**
 - STM32 microcontroller

1. Nucleo F401RE



2. STEVAL-IME014V1



3. STEVAL-IME014V1D



STHV748S

4 channel pulser

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Monolithic 4 channel, 5 level, high voltage pulser

- Pinout compatibility with best selling STHV748
- 0 to $\pm 90V$ output voltage
- Up to 20MHz operating frequency
- PW operation:

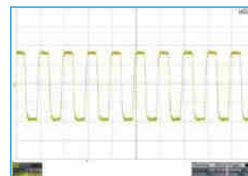
- 3/5-level output waveform
- ± 2 A source and sink current
- ≤ 20 ps jitter

Continuous wave (CW) operation:

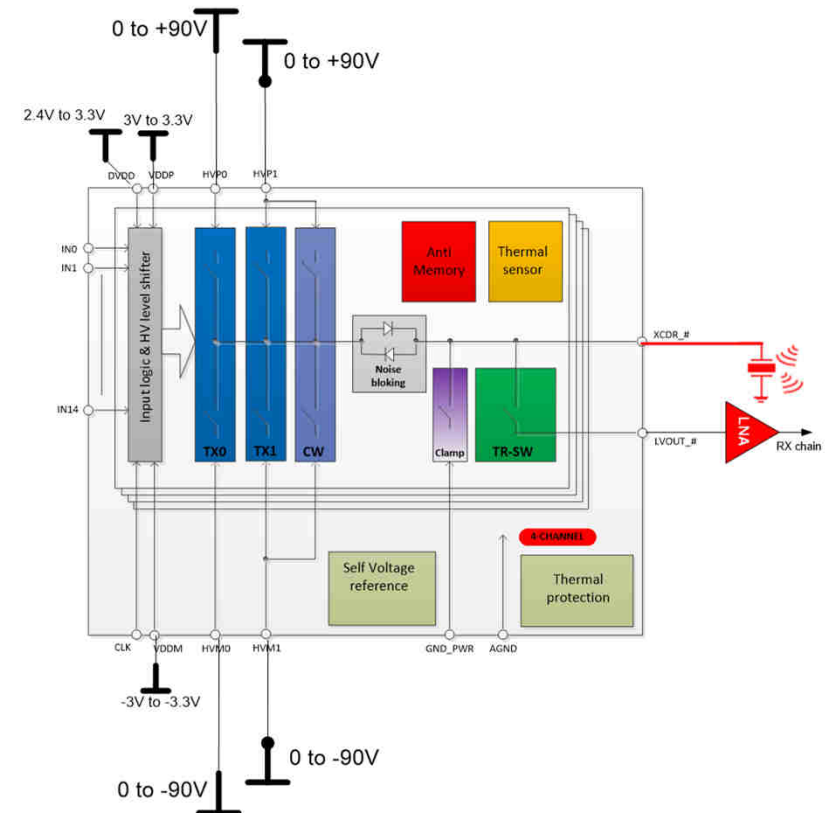
- ≤ 0.1 W power consumption
- ± 0.6 A source and sink current
- 205 fs RMS jitter [100 Hz-20 kHz]
- Integrated 8 Ω synchronous active clamp
- Integrated T/R switch
 - 13.5 Ω on-resistance
 - Up to 300 MHz BW
 - Receiver multiplexing function
- 1.8V to 3.6V CMOS logic interface
- Package: QFN64 9X9 mm



CW mode



5 level PW mode



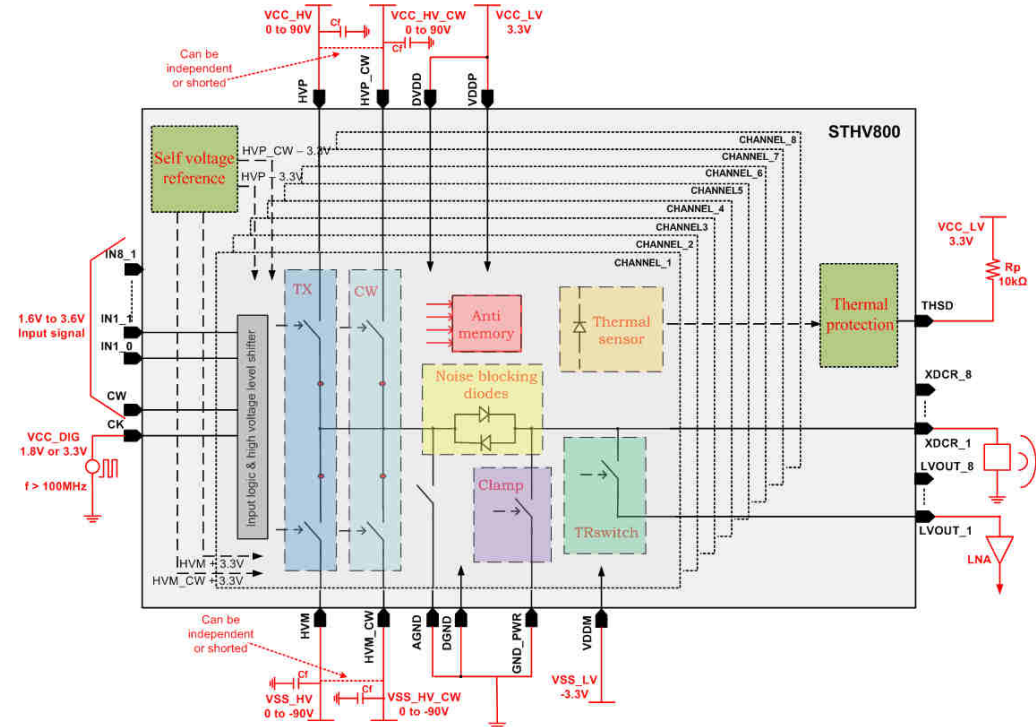
STHV800

8 channel pulser

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Monolithic 8 channels, 3 level, high voltage pulser

- Up to $\pm 90\text{V}$ output voltage
- Up to 20MHz operating frequency
- Two independent half-bridges per channel, one dedicated to continuous wave (CW) mode
- Main half bridge ($\pm 2\text{A}$ source and sink current, 20ps jitter)
- CW half bridge ($\pm 0.3\text{A}$ source and sink current, 10ps jitter)
- Integrated T/R switches (8Ω , 300MHz BW)
- Integrated active clamp switches (8Ω , $\pm 2\text{A}$)
- 6 capacitors integrated in the package
- Power up free
- Current consumption down to $10\mu\text{A}$ in RX phase
- Anti memory function
- 1.8V to 3.6V CMOS logic interface
- Package: LGA 8X8 mm – 56 leads



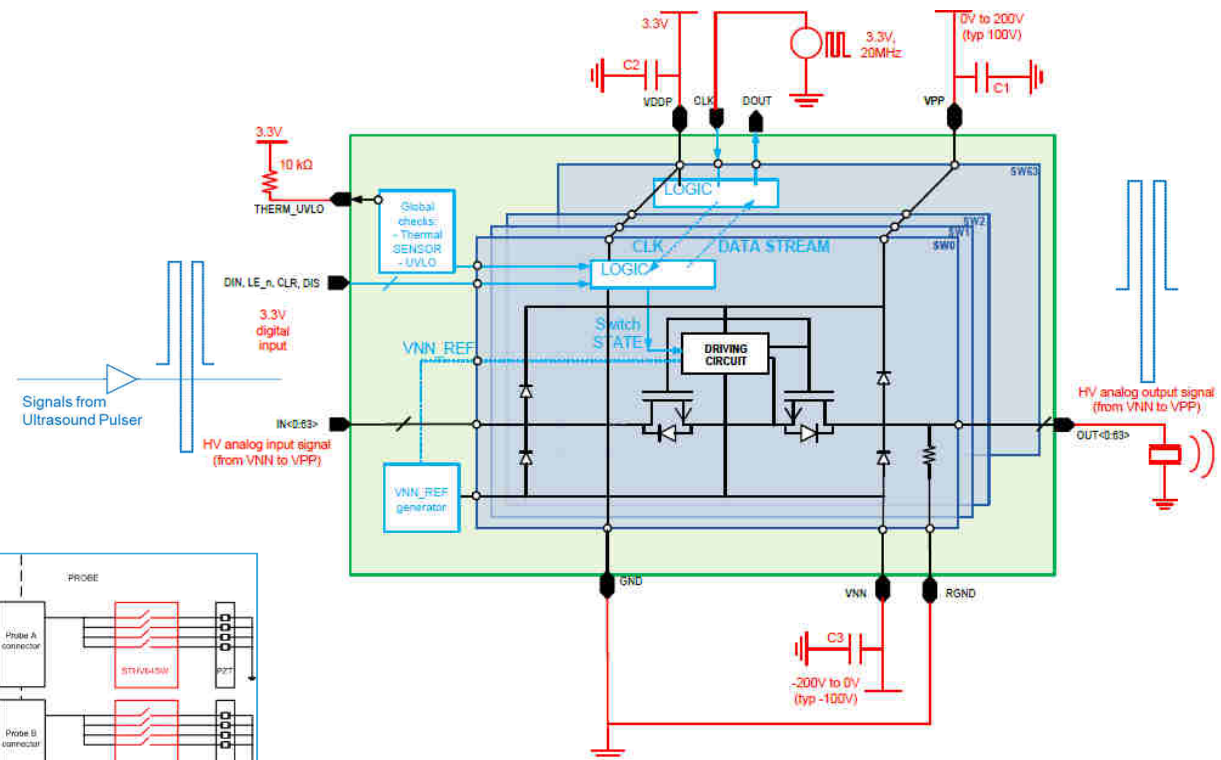
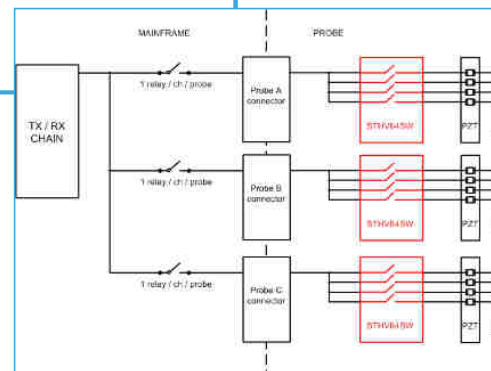
STHV64SW

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64 channel HV Switches

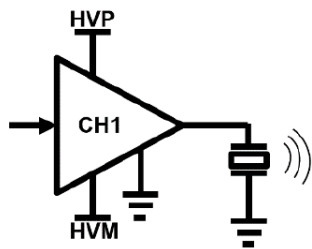
Monolithic 64 independent High Voltage Analog Bi-directional Switches

- 200 V peak-to-peak input and output signal
- Three main operating ranges:
 - From -100 V to +100 V
 - From 0 V to 200 V
 - From -200 V to 0 V
- ± 3 A peak output current.
- Very fast input slew rate (40V/ns at no load)
- Low on-resistance (100 Ω)
- Low cross-talk between channels
- 40k Ω bleed resistor on the outputs
- Recirculation current protection on input and output
- Control through serial interface
- 20 MHz data shift clock frequency
- TFBGA196 12x12

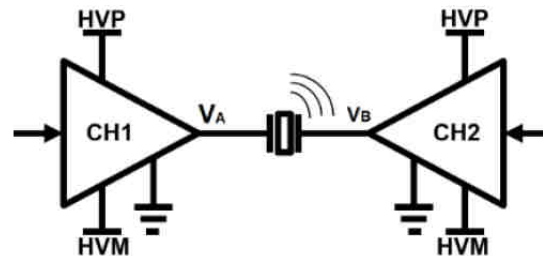


Differential drive for very high voltage

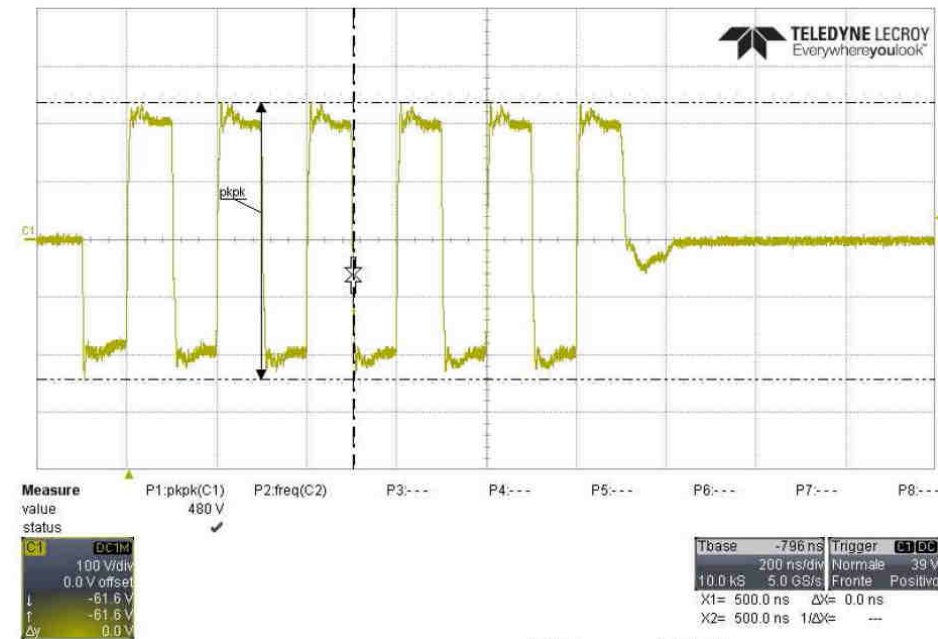
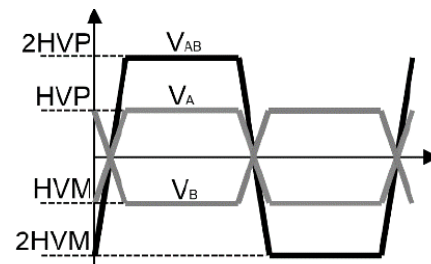
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Single ended drive



Differential drive with two pulsers



400Vpp differential pulsed wave with two channels supplied at +/- 100V

Ultrasound Imaging

ST Key Differentiators

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Customized BCD8SOI technology, optimized for ultrasound

3/5/7/9 output levels to
enhance image quality

Integrated T/R switch and
Beamforming

Very low 10ps jitter for
accurate frequency
response in echo-doppler

Very short 5ns HV pulse
piezo transducer control,
for superior image quality

ST Vision

Towards higher integration

